

Heart Rate Variability Analysis During Weaning from Mechanical Ventilation: Models for Prediction of the Weaning Trial Outcome

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Abstract

This study estimates the activity of the autonomic cardiac control (ACC) in patients undergoing weaning from mechanical ventilation, aiming to predict the weaning outcome. ECG and AVEA ventilator data from 13 successfully and 14 unsuccessfully weaned patients were collected. Heart rate variability (HRV) profiles were estimated in non-sedated patients during 2 weaning phases: (1) PSV - pressure support ventilation at 12-25 cmH₂O; (2) SBT – spontaneous breathing trial at 8 cmH₂O. HRV indices in the time- and frequency-domain were analyzed on 5-min RR-interval episodes under stationary conditions during each weaning phase.

Our model for prediction of the successful weaning outcome considers 3 basic mechanisms for adequate ACC response on the weaning cardio-respiratory stress: (1) preserved ACC ability to maintain physiological adaptation; (2) modulated ACC activity by the breathing model; (3) mostly neurohumoral regulation of the blood circulation. The successful group model exhibits reduced total activity (TP, SDNN) with increased sympathetic (VLF/TP, LF/HF>1) and reduced vagal tone (HF/TP, RMSSD, pNN50), the latter correlated to the respiratory rate and tidal volume. Deviations from this HRV model are indicative for weaning failure detected with accuracy 92.6% (PSV), 81.5% (SBT), 96.3% (SBT-PSV).

1. Introduction

Mechanical ventilation (MV) of critically ill patients is associated with many risks and complications that lead to high morbidity, mortality, longer intensive care unit stay, and higher treatment costs [1]. Identifying the patient's readiness at the earliest time possible for successful weaning from MV is the primary target for patients with command breathing [2]. Discontinuation from MV is the process for a gradual reduction in ventilator support, to allow patients the ability to assume increasing levels of work to breathe until sustain spontaneous breathing. This

weaning process occupies an average of 40% of the total duration of mechanical ventilation, with failure in over one third of MV patients. The consolidated evidence-based clinical practice guidelines of the American Thoracic Society (ATS) and the American College of Chest Physicians (CHEST) point out the process of MV liberation as an investigation priority [1].

Weaning from MV has impact on the cardiovascular function by 3 physiological mechanisms [3-6]:

- 1) Changes in the oxygen transport (hypoxia), which may provoke circulatory disturbances with a terminal result of weaning failure or other fatal complications (acute myocardial infarction, heart failure and cardiogenic pulmonary edema, rhythm disorders).
- 2) Haemodynamic alterations as a result of changes in the intrathoracic pressure (ITP), which is positively dependent on the tidal volume and modulated by MV breathing cycles [6]. The associated changes in the cardiac output, ventricular preload and afterload may result in acute alterations of cardiac mechanics and myocardial ischemia, manifested as arrhythmias.
- 3) Effects on the autonomic nervous system (ANS) activity, which is influenced by humoral changes in the intrathoracic cardiovascular system due to ITP changes. Therefore, ANS tries to compensate for these humoral changes by two mechanisms – increasing the sympathetic tone and decreasing the parasympathetic tone that affects the heart rate.

Heart rate variability (HRV) is the physiological phenomenon of inter-beat interval variation due to the joint action of the sympathetic and parasympathetic parts of the autonomic cardiac control (ACC) [7]. A number of studies on HRV changes at different phases during MV discontinuation have concluded that ACC status provides essential information on the pathophysiological imbalances reflected in the success or failure of weaning [3-5,8-14]. In failure patients, reduced HRV and vagal tone withdrawal have been reported [9,10,12]. This study aims to derive models for prediction of the weaning outcome by HRV, breathing and metabolic features, and to better understand the ACC role during MV weaning.

2. Materials and methods

2.1. Study population

Data from 27 patients undergoing weaning from MV (63% men, age 58±17 years, Simplified Acute Physiology Score SAPS II = 28.9±8.2) were collected with AVEA ventilator system in the intensive care unit of the Pirogov University Emergency Hospital, Sofia. According to inclusion criteria, the enrolled patients did not have cardiac arrhythmias, neurological diseases, did not take pre-medication with cardiovascular drugs, and received CMV for at least 72 hours prior to the study. The decision to start weaning and weaning outcome has been made by the primary care physician following a weaning protocol approved by the local Ethics Committee, in concord to general weaning and extubation criteria [15].

The study considered two weaning phases in non-sedated patients:

- 1) Pressure support ventilation (PSV): titration of the inspiratory pressure support level from 25 down to 12 cmH₂O during about 30 min. All patients have successfully passed this phase.

- 2) Spontaneous breathing trial (SBT): PSV at 8 cmH₂O. SBT was terminated if the patient exhibited signs of poor tolerance.

The weaning outcome was estimated by the ability of the patient to maintain the SBT challenge for at least 2 hours, being successful (S=13 patients) and failed (F=14 patients).

2.2. HRV analysis

ECG signal (lead I, 500Hz) was continuously recorded. Time series of normal-to-normal RR-intervals (NN), deduced from adjacent normal sinus beats in stable artifact-free 5-min episodes under stationary conditions were extracted after the beginning of PSV and SBT. Standardized HRV indices [7] were calculated (Table 1):

- TIME-HRV from the time-domain NN-tachogram, dNN-tachogram (NN-intervals first differences) and NN-histogram (using standard discrete scale resolution of the bin equal to 7.8ms=1/128Hz).

- FREQ-HRV. Fourier Transform of NN interval time series resampled at 4Hz was applied to derive the power spectrum density components of HRV.

Table 1. Mean±standard deviation of time-frequency domain HRV, ventilatory and hemodynamic indices for failure (F=14 patients) and successful group (S=13 patients) during PSV and SBT. *: p<0.05 comparing F vs. S groups by T-test.

| Measurements | PSV | | SBT | | SBT-PSV | | |
|-------------------------------|---|-----------------|-----------------|----------------|----------------|---------------|----------------|
| | Success | Failure | Success | Failure | Success | Failure | |
| TIME-HRV | HR (bpm) = 60/mean of NN-intervals | 100±19 | 94±23 | 101±19 | 95±22 | 0.7±7.5 | 1.7±3.3 |
| | SDNN (ms): std. deviation of NN-intervals | 18±12 | 19±27 | 17±15 | 20±23 | 0.8±8.3 | 1.2±6.3 |
| | MDNN (ms): mean deviation of NN-intervals | 14±10 | 14±22 | 13±12 | 15±19 | 0.2±7 | 0.5±5 |
| | SDNNd (ms): std. deviation of dNN | 8±10 | 12±15 | 9±14 | 13±16 | 2.4±5.1 | 1.2±3.6 |
| | MDNNd (ms): mean deviation of dNN | 4±6 | 8±12 | 6±10 | 8±12 | 1.9±4.7 | 0.4±2.9 |
| | pNN50 (%): proportion of dNN>50ms | 1.0±3.2 | 5.4±14.5 | 2.1±6.6 | 5.5±15.8 | 1.1±3.5 | 0.1±3.5 |
| | RMSSD (ms): root-mean square of dNN | 10±11 | 17±23 | 12±16 | 19±25 | 3.4±6.5 | 1.9±5.3 |
| | TRI: triangular index of NN-histogram | 4.6±2.9 | 4.4±4.9 | 3.7±2.3 | 4.4±4.3 | -0.5±0.8 | 0.1±1.2 |
| FREQ-HRV | TP (ms ²): total power (0.015-0.4 Hz) | 154±263 | 527±1593 | 207±369 | 546±1786 | 112±275 | 19±248 |
| | VLF/TP (%): very low freq. (0.015-0.04 Hz) | 53±17* | 31±19* | 47±23 | 37±25 | -5±13* | 6.8±15* |
| | LF/TP (%): low freq. band (0.04-0.15 Hz) | 27±7 | 28±14 | 27±13 | 26±13 | -1.9±11 | -2.6±11 |
| | HF/TP (%): high freq. band (0.15-0.4 Hz) | 20±15* | 41±26* | 26±23 | 37±29 | 6.9±14 | -4.2±20 |
| | LF/HF ratio | 3.3±2.6* | 1.4±1.5* | 3.6±4.2 | 1.9±2.1 | -0.04±1.7 | 0.4±1.6 |
| AVEA Ventilator (VENT) | SYS (mmHg): systolic blood pressure | 126±20 | 138±27 | 133±24 | 147±36 | 8±19 | 8.4±17 |
| | DIA (mmHg): diastolic blood pressure | 67±10 | 76±17 | 74±11 | 79±24 | 5±9 | 3.5±9.4 |
| | SpO2 (%): oxygen saturation | 97.1±1.8 | 95.9±3.0 | 95.9±2.6 | 93.7±3.4 | -1.1±2.9 | -2.1±2.5 |
| | f (br/min): breathing frequency | 18±6 | 23±8 | 27±6* | 34±7* | 9±4 | 11±8 |
| | Vt (mL): tidal volume | 542±120* | 423±130* | 379±92* | 288±91* | -169±101 | -136±113 |
| | MV (L/min): minute volume | 8.7±2.5 | 8.5±2.2 | 9.7±2.8 | 10.0±2.5 | 0.4±1.1 | 1.4±2.4 |
| | RSBI=f/Vt: rapid shallow breathing index | 37±24* | 63±32* | 76±26* | 133±56* | 40±21* | 70±44* |
| | PETCO2 (mmHg): end-tidal carbon dioxide | 35±8 | 34±8 | 32±6 | 33±7 | -1.7±3.2 | -0.6±3.0 |
| | VO2 (mL): oxygen consumption | 275±68 | 294±94 | 311±65 | 390±124 | 36±48 | 96±95 |
| | VCO2 (mL): carbon dioxide elimination | 213±56 | 231±74 | 231±44 | 250±83 | 17±35 | 19±33 |
| | RQ: respiratory quotient | 0.75±0.09 | 0.72±0.12 | 0.74±0.11 | 0.67±0.1 | -0.01±0.1 | -0.05±0.1 |
| EE (kCal): energy expenditure | 1907±559 | 1949±520 | 2064±513 | 2316±673 | 177±270 | 367±633 | |

2.3. Weaning outcome prediction model

Both HRV indices and AVEA ventilator measurements (Table 1) were processed in Matlab (MathWorks, Inc.) by forward stepwise linear discriminant analysis (SDA) to derive models for prediction of the weaning outcome. Models using different input vectors were trained, aiming to select the most powerful and non-redundant predictors, measurable during PSV, SBT, and the difference (SBT-PSV). The feature selection process was iterative, so that at each step, SDA was forced to include the predictor, which led to maximal classification accuracy:

$$Accuracy = \frac{TP + TN}{TP + FN + TN + FP},$$

where TP, FN are true positives and false negatives for detection of the weaning failure group (F=14 patients); TN, FP are true negatives and false positives for detection of the weaning success group (S=13 patients).

Leave-one-out cross-validation was applied to derive the maximal classification accuracy achieved by SDA. Moreover, to avoid overtraining on the small size database, SDA was limited to include up to 7 features or the training stopped while reaching a plateau in the accuracy step-up trend for >2 steps.

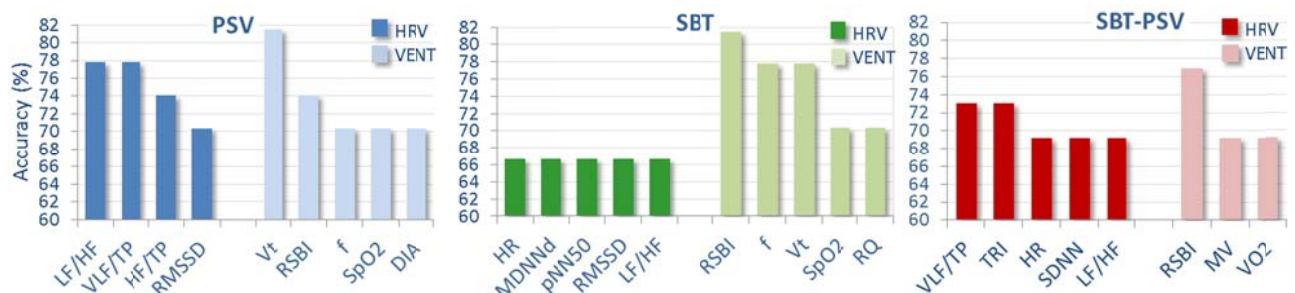


Figure 1. Top-ranked features (HRV, breathing, metabolic) in PSV, SBT, SBT-PSV for prediction of the weaning outcome.

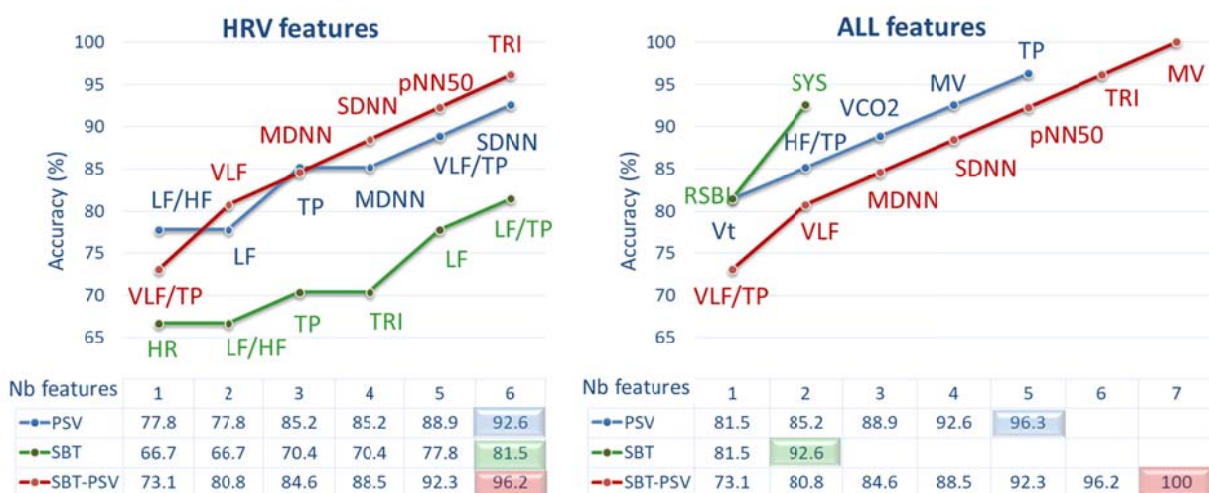


Figure 2. Performance of 6 SDA models for prediction of the weaning outcome, showing the iteratively selected features (only HRV – left graph, all features – right graph) in PSV, SBT, SBT-PSV that lead to maximization of accuracy.

3. Results and discussion

The mean value dispersion (Table 1) of linked FREQ-HRV and TIME-HRV features provide reliable evidence for the cardiac autonomic balance (CAB) interpretation:

- Vagal activity is 1.6 to 5-fold higher in Failure patients, confirmed by the comparison (F vs. S) of:
 - HF/TP: 41% vs. 20% (PSV), 37 vs. 26% (SBT)
 - pNN50: 5.4% vs. 1% (PSV), 5.5% vs. 2.1% (SBT)
 - RMSSD: 17 vs. 10 ms (PSV), 19 vs. 12 ms (SBT).
- Sympathetic activity is 1.3 to 2.4-fold higher in Successful patients, confirmed by comparison (S vs. F) of:
 - VLF/TP: 53% vs. 31% (PSV), 47% vs. 37% (SBT)
 - LF/HF ratio: 3.3 vs. 1.4 (PSV), 3.6 vs. 1.9 (SBT)
 - LF/TP is indifferent to the weaning outcome (26-28%), representing mixed sympathetic and vagal activity. LF is not appropriate as a marker of the sympathetic tone, as widely interpreted [8-10,13].
- Sympathovagal balance during PSV to SBT transition shows different ACC reaction:
 - Failure patients become more stressed (VLF increases by 6.8%, HF decreases by 4.2%).
 - Successful patients become more relaxed (VLF decreases by 5%, HF increases by 6.9%).

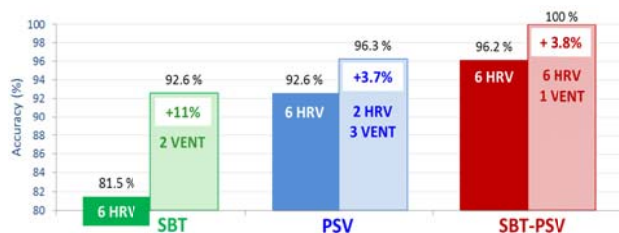


Figure 3. Final model for prediction of the weaning outcome: accuracy, number and type of included features.

The above analysis provides evidence that patients who succeed and failed during the weaning process have important differences in the ANS regulation:

- 1) Successful patients have prevalently sympathetic modulation, also confirmed in [8,11]. They maintain:
 - *Physiologic adaptation* to the cardio-respiratory stress, immediately after the beginning of PSV.
 - *Intensive sympatho-adrenal stimulation* to return the normal circulation (VLF \uparrow)
 - *HRV modulation by the breathing pattern* (HF \downarrow , LF/HF \uparrow when f \uparrow , Vt \downarrow).
- 2) Failure patients keep high tension of the autonomic contour. They manifest:
 - *Increased vagal tone* (HF \uparrow , LF/HF \downarrow) and *considerable HRV* (TP \uparrow , SDNN \uparrow) during PSV, SBT.
 - *Slow physiologic adaptation*:
 - Later trend to increase of the sympathetic activity (*transition PSV to SBT*).
 - This phenomenon was interpreted in some studies as “*vagal tone withdrawal*” [9,10,12].

In this study, we stress the importance of the following HRV features to the prediction of the weaning outcome:

- *VLF component*, distinguishing the neurohumoral regulatory mechanisms during MV weaning [3]. The incomplete *FREQ-HRV* model (TP=LF+HF) in many studies [8-10,13] is deficient, also confirmed by the observed LF invariance to the weaning outcome.
- Both *TIME-HRV* and *FREQ-HRV* analyses provide the ground for reliable CAB activity interpretation by established strong correlations between pairs of time- and frequency-domain HRV indices. Study of only time-domain HRV [3] or highly variable frequency-domain HRV (mainly LF and HF) [9-11,13,14] can lead to interpretation bias, e.g. considering the effect of LF saturation at significant sympathetic ACC tone.

The prognostic value of HRV to the weaning outcome is significant, comparable to the breathing pattern features. The most powerful models are shown to be:

- 1) HRV-features (Figures 1-3):
 - PSV (LF/HF or VLF/TP) = 78%
 - SBT-PSV (6 HRV features) = 96.2%
- 2) Ventilator VENT-features (Figure 1):
 - PSV (Vt), SBT (RSBI) = 81%
- 3) All features: HRV + VENT (Figures 2, 3):
 - SBT-PSV (6 HRV + 1 VENT) = 100%.

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