

Effects of the β -Adrenoceptor Blocker Carvedilol in Short QT Syndrome Caused by N588K Mutation in HERG: A Simulation Study

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Abstract

The short QT syndrome (SQTS) is associated with shortening of QT interval resulting from an accelerated cardiac repolarization. The SQT1, SQTS variant, results from a gain-of-function N588K-KCNH2 mutation in the rapid delayed rectifier potassium current (I_{Kr}) channels. Since β -Adrenoceptor blocker can block slow delayed rectifier potassium currents (I_{Ks}) and I_{Kr} , we used *in silico* approach to evaluate carvedilol's effects on SQT1.

Mathematical models of human ventricular action potential (AP) developed by ten Tusscher *et al.* were modified to incorporate a Markov chain formulation of I_{Kr} describing the SQT1 mutant condition. AP models were incorporated into a transmural strand for investigation of QT interval changes. In addition, the simulated I_{Ks} and I_{Kr} inhibition to prolong the QT interval in SQT1 was quantified. The blocking effects of carvedilol on I_{Ks} and I_{Kr} were modelled by using Hill coefficient and IC_{50} from literatures (10 μ M carvedilol reduced I_{Kr} in Wild Type- and N588K-KCNH2 by 92.8% and 36.0%; it reduced I_{Ks} by 36.5% in both conditions). At single cell level, carvedilol prolonged the AP duration (APD) in SQT1; at strand level, the effects of carvedilol normalized the QT interval in SQT1 from 286 ms to 364 ms.

Simulations identified β -Adrenoceptor blocker carvedilol as a potential drug for SQTS treatment.

1. Introduction

The short QT syndrome (SQTS) is a cardiac disorder associated with abnormally short QT interval on the ECG, leading to increased risk of atrial and/or ventricular arrhythmias and sudden cardiac death [1,2]. The SQTS is

genetically heterogeneous, with a complex genotype-phenotype relationship. The first identified form of the SQTS (SQT1) [3] was caused by a missense mutation (N588K) to the human *hERG* encoding the channels carrying the rapid delayed rectifier potassium current, I_{Kr} . Studies [2,4] showed the N588K-*hERG* mutation significantly attenuated inactivation, without altering the voltage dependence of activation, causing a "gain-of-function" in I_{Kr} which significantly reduces the QT interval ($QTc \leq 300$ ms).

The current first-line treatment for SQTS patients is use of an implantable cardioverter-defibrillator (ICD) device, which protects against SCD [5]. However, T-wave over-sensing, which leads to erroneous identification of tachyarrhythmic events, can be an issue with such devices, as T-waves often appear tall and peaked in SQTS patients. Furthermore, ICD does not restore the QT interval and, is not suited to some pediatric patients, necessitating the pursuance of alternative, pharmacological approaches. Pharmacological therapy may be the primary modality to restore the physiological (normal) QT interval and protect against arrhythmias. At present, the accurate experimental models of SQT1 and *in vitro* pharmacological data on SQT1 patients are comparatively sparse [2,4]. However, previous studies have reported that β -adrenoceptor blocker carvedilol has some efficacy in reversing the SQTS phenotype [6]. Detailed *in vitro* studies into the pharmacology of N588K-KCNH2 and V307L-KCNQ1 mutations used patch clamp measurements to assess the blocking potency of β -adrenoceptor blocker carvedilol on I_{Ks} and I_{Kr} currents [6]. In this study, β -adrenoceptor blocker carvedilol emerged as a potential agent for treating SQTS.

The underlying mechanisms by which combined ion

channel blocking actions of carvedilol exert anti-arrhythmic effects in the setting of SQT1 are not known. Whereas, several studies [1,2,7-10] have previously used computer models to gain insights into QT interval shortening and pro-arrhythmic effects of SQT1 mutant *hERG* channels in human ventricles, significantly less is known about the pharmacological agents on human ventricular electrophysiology in SQT1 variant. Our simulation studies adopted a simplified “pore block” approach to investigate the effects of drugs on SQTS [2,10]. The present study was also adopted simplified “pore block” approach to provide mechanistic information regarding the actions of carvedilol on human ventricular electrophysiology in the setting of N588K-linked SQT1.

2. Methods

2.1. Model development

The ten Tusscher model [11,12] of the human ventricular action potential (AP) was used for simulations in this study, due to its extensive experimental validation and ability to reproduce complex behaviours when simulating anti-arrhythmic effects of pharmacological agents on cardiac electrophysiology. An updated form of the ten Tusscher model described by Zhang *et al.* [4] was used, as this configuration gave a QT interval shortening which was more concordant with clinical observed in the SQTS.

Specifically, the single cell model can be modelled by using the following ordinary differential equation (ODE):

$$\frac{dV_m}{dt} = -\frac{I_{ion} + I_{stim}}{C_m} \quad (1)$$

where t is time, C_m is the cell membrane capacitance, I_{stim} is the external stimulus current and I_{ion} is the sum of the transmembrane currents. The late sodium current (I_{NaL}) equation [13] was incorporated. The model code used in this study was downloaded from <http://www-binf.bio.uu.nl/khwjtuss/>. The cell model was paced with an amplitude of -52 pA/pF for 1 ms and a basic cycle length (BCL) of 800 ms.

To simulate the electrophysiological effects of the *KCNH2* N588K mutation, the parameters of I_{Kr} equations were modified to incorporate the experimentally-observed kinetic properties of I_{Kr} channels [4]. As SQTS mutations are expressed heterozygously *in vivo*, and according to our previous work [4], the modified parameters of the I_{Kr} equations are presented below.

Original:

$$I_{Kr} = G_{Kr} \times O_{Kr} \times (V_m - E_{Kr}) \quad (2)$$

$$G_{Kr} = 0.0243 \times [K^+]_o^{0.59} \text{ nS / pF} \quad (3)$$

$$E_{Kr} = \frac{RT}{F} \log \frac{[K^+]_o}{[K^+]_i} \quad (4)$$

WT:

$$\alpha_1 = 2.172 \quad (5)$$

$$\beta_1 = 1.077 \quad (6)$$

$$\alpha_2 = 0.00655 \times e^{0.027735765 \times (V-36)} \quad (7)$$

$$\beta_2 = 0.001908205 \times e^{0.0148902V} \quad (8)$$

$$\alpha_i = 0.04829 \times e^{-0.039984 \times (V+25)} \times \left(\frac{4.5}{K_o}\right) \quad (9)$$

$$\beta_i = 0.2624 \times e^{0.000942V} \times \left(\frac{4.5}{K_o}\right)^{0.3} \quad (10)$$

$$\alpha = 0.00555 \times e^{0.05547153 \times (V-12)} \quad (11)$$

$$\beta = 0.002357 \times e^{-0.036588V} \quad (12)$$

$$\mu = \frac{\alpha_i \beta_2}{\beta_i} \quad (13)$$

N588K:

$$\alpha_1 = 2.172 \quad (14)$$

$$\beta_1 = 0.5385 \quad (15)$$

$$\alpha_2 = 0.001965 \times e^{0.05547153 \times (V-21)} \quad (16)$$

$$\beta_2 = 2.260489 \times 10^{-6} \times e^{-0.0925782V} \quad (17)$$

$$\alpha_i = 0.439 \times e^{-0.02352 \times (V+40)} \times \left(\frac{4.5}{K_o}\right) \quad (18)$$

$$\beta_i = 0.0164 \times e^{0.000942 \times (V+15)} \times \left(\frac{4.5}{K_o}\right)^{0.3} \quad (19)$$

$$\alpha = 0.00555 \times e^{0.05547153 \times (V+3)} \quad (20)$$

$$\beta = 0.002357 \times e^{-0.036588V} \quad (21)$$

$$\mu = \frac{\alpha_i \beta_2}{\beta_i} \quad (22)$$

A scaling factor ratio of 1.5: 1 in epicardial (EPI) I_{Ks} to mid-myocardial (MIDDLE) I_{Ks} , was applied as reported in the study of Szabo *et al.* [14], in order to generate a high, symmetrical T-wave.

2.2. Drug effect modelling

Simplified ‘‘pore block’’ [15] was used for drug modelling. The effects of carvedilol on I_{Kr} , I_{Ks} , were described using Hill coefficient (nH) and half maximal inhibitory concentration (IC_{50}) values taken from the literature (10 μ M carvedilol reduced I_{Kr} in Wild Type- and N588K-*KCNH2* by 92.8% and 36.0%; it reduced I_{Ks} by 36.5% in both conditions) [6].

2.3. Tissue Simulation

The mono-domain equation was used to describe the initiation and conduction of APs in the multi-cellular tissue, which is described by the following partial differential equation (PDE):

$$C_m \frac{\partial V_m}{\partial t} = -(I_{ion} + I_{stim}) + \nabla \cdot (D \nabla V_m) \quad (23)$$

where D is the diffusion coefficient tensor. Equation (23) was solved numerically using a finite-difference PDE solver based on the explicit forward Euler method, as described previously.

We constructed a 15 mm strand model, and employed a spatial resolution of 0.15 mm. It had 25 nodes for ENDO, 35 nodes for MIDDLE and 40 nodes for EPI cells. D was set at 0.0008 cm^2/ms , which promoted a conduction velocity (CV) of 52 cm/s.

A pseudo-ECG was calculated by the following expression [16]:

$$\phi_e(x') = \frac{\alpha^2}{4} \int (-\nabla V_m) \cdot \nabla \left(\frac{1}{r}\right) dx \quad (24)$$

The virtual electrode was placed at a position 2.0 cm away from the EPI end of the strand.

3. Results

Figure 1 shows the simulated cell APs with the modified I_{Kr} equations. These plots show cell AP V (mV) versus time t (ms), stimulated by a 1.25 Hz frequency. Carvedilol prolonged the AP duration in the SQT1 condition.

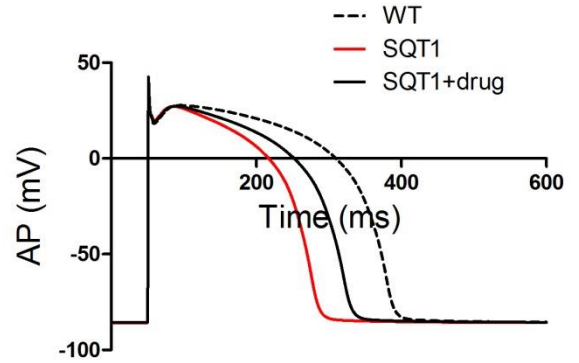


Figure 1. The pharmacological effects of carvedilol on cell action potentials in SQT1 conditions.

A pseudo-ECG was simulated by using a strand model as shown in Figure 2. The QT interval on the ECG was prolonged in SQT1 condition by the application of 10 μ M carvedilol. It normalized the QT interval in SQT1 from 286 ms to 364 ms.

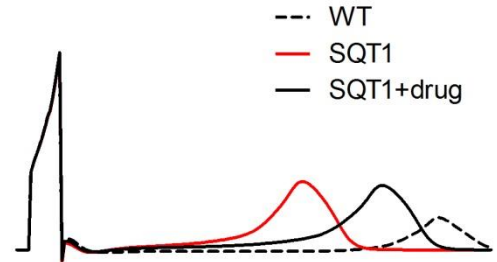


Figure 2. The pharmacological effects of carvedilol on pseudo-ECGs in SQT1 conditions.

4. Conclusion

In the present study, we have showed that 10 μ M β -adrenoceptor blocker carvedilol produced a therapeutic effect on ventricular electrophysiology in SQT1 conditions, which identified as a potential drug of choice for SQTs treatment.

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