# Ranolazine Attenuates Stretch-induced Modifications of Electrophysiological Characteristics in HL-1 cells

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#### Abstract

Mechanical stretch induces an increase in  $Na^+$  influx into myocytes, related to mechanisms including stretchactivated channels or activation of Na+/H+ exchanger, involving changes in electrophysiological properties favouring arrhythmia induction. The aim of this study is to investigate the effects of mechanical stretch in cultured atrial murine cells (HL-1 myocytes) and its pharmacological response to ranolazine.

Confluent HL-1 myocytes with spontaneous fibrillatory activity was cultured in silicone membrane plates, and were stretched to 110% of resting length. The response to stretch under control conditions and under ranolazine effects was analyzed using a high-resolution optical mapping system.

HL-1 cells stretching increased atrial fibrillation dominant frequency in control conditions. The administration of ranolazine reduced this stretch-induced effect, and slowed the arrhythmia in baseline conditions.

Ranolazine attenuates the modifications of electrophysiological effects induced by myocardial stretch in HL-1 cells model of AF.

#### 1. Introduction

Mechanical stretch is the common final stimulus to atrial myocytes in various cardiovascular diseases that are associated with atrial fibrillation (AF), such as mitral valvular disease, hypertension, and congestive heart failure [1]. Mechanical stretch induces an increase in Na<sup>+</sup> influx in myocytes, related to mechanisms including stretch-activated channels or activation of Na<sup>+</sup>/H<sup>+</sup> exchanger, and activates the reverse mode of Na<sup>+</sup>/Ca<sup>2+</sup> exchanger, involving changes in electrophysiological properties favouring arrhythmia induction [2,3]. An increase in Na<sup>+</sup> current due to an increased number of active channels has also described as an expression of mechanosensitivity of the voltage-gated sodium channel Na<sub>v</sub>1.5 [4], which activation could enhance the persistent or late sodium inflow (I<sub>NaL</sub>) through the plateau of the action potential [5]. Moreover, I<sub>NaL</sub> current is also activated by the stretch-induced increase of intracellular Ca<sup>2+</sup> concentration [5].

Ranolazine is an antiaginal agent that has been shown to exert a protective effect against cardiac arrhythmias linked to the enhancement of  $I_{NaL}$  current and cellular  $Ca^{2+}$  overload [6]. The effects of ranolazine and the reduction of Na<sup>+</sup> entry into myocytes could modulate the electrophysiological effects of stretch.

The purpose of this work is to investigate the effects of mechanical stretch on electrophysiological characteristics during atrial fibrillation in cultured atrial myocyte monolayer in order to assess the effect of ranolazine and to determine whether it could modify the electrophysiological effects of stretch.

#### 2. Material and methods

# 2.1. Cell culture

HL-1 cells were maintained, grown and proliferated according to the standard protocol established by Claycomb et al. [7] in 2x2 flexible PDMS wells.

# 2.2. Experimental protocol

After achieving further cell confluency, HL-1 cells spontaneous presented fibrillatory activity [8]. It has been reported that HL-1 cells are a viable in vitro model for study of the effects of mechanical stimulation on electrical characteristics [1]. In order to evaluate the effects of mechanical stretch on AF characteristics, myocytes were stretched in a strain unit to 110% of resting length for 10 minutes, and after this period stretch

was supressed (Fig. 1). For each situation (basal, stretch, post-stretch), optical mapping recordings of fibrillatory activity were acquired under control conditions and after the administration of ranolazine (50  $\mu$ M in Tyrode solution).

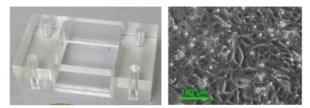


Figure 1. Confluent HL-1 murine monolayer in 2x2 polysimethylsiloxane (PDMS) membrane plates

# 2.3. Optical mapping

Calcium transient (CaT) imaging was developed by means of a high-resolution optical mapping system, and results were further analyzed by custom software developed in MATLAB [8].

Power spectra of optical signals were estimated by using Welch periodogram (2-s Hamming window overlap). Dominant frequency (DF) of each pixel was determined as the frequency with the largest peak in the spectrum between 0.05 and 30 Hz. For each individual cell culture, the highest DF was defined as the maximum DF of the entire dish.

#### 2.4. Statistical analysis

The previously analysis was performed in 12 monolayers of fibrillating HL-1 cells. Data are presented as mean  $\pm$  standard deviation. Continuous variables were compared using repeated measures ANOVA test or Wilcoxon and Friedman's tests, depending on the variable's statistical distribution.

#### 3. Results

In all 12 analyzed cell cultures, AF was stable along the protocol duration. CaT maps of a representative example of each situation are shown in the figure 2.

# **3.1. Effects of ranolazine on baseline activation patterns during AF**

During baseline recordings (prior to stretch) dominant frequency was significantly smaller under ranolazine perfusion than in control conditions  $(3.04 \pm 0.18 \text{ Hz vs.}$  $3.65 \pm 0.20 \text{ Hz}$ , p<0.01) (Fig. 3), where the slowing effect of the drug is evident. After supressing stretch, ranolazine reduces frequency activation slowing the arrhythmia  $(3.00 \pm 0.24 \text{ Hz vs.} 3.63 \pm 0.31 \text{ Hz}, p<0.05)$  (Fig. 3).

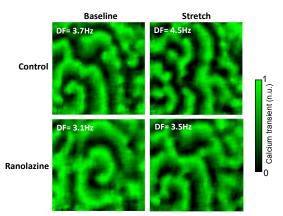


Figure 2. CaT maps of representative cell cultures in basal (left) and stretch (right) situations, during control conditions (top) and after the administration of ranolazine (bottom).

# **3.2.** Effects of ranolazine on stretchinduced modifications of activation patterns during AF

In control series, DF increased significantly during stretch  $(3.65 \pm 0.20 \text{ Hz vs.} 4.35 \pm 0.23 \text{ Hz})$  and returned to baseline values after stretch suppression  $(3.63 \pm 0.31 \text{ Hz})$  (Figure 3). The magnitude of stretch-induced DF increment was 19.7%.

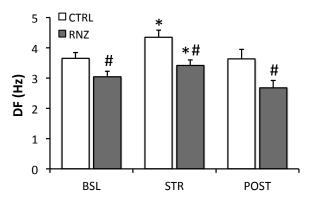


Figure 3. Dominant frequency in control and ranolazine conditions, for basal, stretch and post-stretch situations. \*p vs. BSL, #p vs. CTRL.

The administration of ranolazine attenuated the electrophysiological effects of stretch. Under ranolazine action, stretch-induced DF increasing remained ( $3.04 \pm 0.18$  Hz vs.  $3.42 \pm 0.18$  Hz, p<0.05), but was reduced (Fig. 3). In fact, the magnitude of DF increment was smaller under ranolazine effects than in control conditions (12.4% vs. 19.7%, p<0.01) (Fig. 4).

Moreover, stretched cell cultures treated with ranolazine presented lower dominant frequencies  $(3.42 \pm 0.18 \text{ Hz vs. } 4.35 \pm 0.23 \text{ Hz}, \text{ p} < 0.01)$  (Fig. 3).

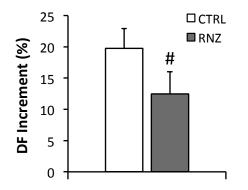


Figure 4. Increment of dominant frequency in control and ranolazine conditions after stretching. #p<0.01 vs. CTRL.

#### 4. Discussion

In the present study, we have used an experimental model involving HL-1 cells monolayer in which the analysis of the spectral characteristics of myocardial activation during atrial fibrillation allow us to track the time course of the electrophysiological changes induced by stretch. The study was carried out to analyze the effects of ranolazine on the electrophysiological responses induced by mechanical stretch.

In the absence of stretch, we observed a slowing effect on activation during AF by ranolazine. Dominant frequency was lower under drug action, effect associated to an increase in refractoriness. In this situation, rather than by block of late Na<sup>+</sup> current which would shorten repolarization, the increase of refractoriness would be due to block of repolarizing  $I_{Kr}$ , known effect for ranolazine (IC50  $\approx 10 \,\mu$ M).

In the present work, as in previous studies on isolated Langendorff-perfused rabbit hearts [9], we found that stretch increased the AF dominant frequency, which can be considered as proarrhythmic.

The stretch-induced changes on HL-1 activation were attenuated under the action of ranolazine. Dominant frequency increments under stretch were smaller under ranolazine effect and we observed a reduction in the activation rate, which can be considered as antiarrhythmic. These results support the hypothesis that this  $I_{NaL}$  blocker could modulate cardiomyocyte mechanosensitivity and suggest that other protective effects of ranolazine may be involved.

A factor that may be related to the effects of ranolazine during HL-1 cells stretch is the action of the drug upon stretch-induced modulation of  $Na_v 1.5$ . The the mechanosensitivity of Nav1.5 consists of accelerated kinetics, an increased peak current, and stabilization of inactivation In fact. modulation of [1]. mechanosensitivity of Nav1.5 has been demonstrated at high ranolazine concentrations (50  $\mu$ M), though the drug effects depend on the magnitude of stretch and on the ranolazine membrane concentration [1].

Finally, aside from  $Na_v 1.5$  and  $I_{NaL}$ , ranolazine inhibits other ionic currents as  $I_{CaL}$  and  $I_{Na-Ca}$ , which are some of the mechanisms involved in the effects of stretch [6,9]. Nevertheless, the inhibition of these currents was weak at atrial level for the concentration used in this work [6].

#### 5. Conclusion

Ranolazine attenuates the electrophysiological effects responsible for the acceleration of AF induced by myocardial stretch in HL-1 cells.

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